

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property
Organization
International Bureau



(43) International Publication Date
15 January 2004 (15.01.2004)

PCT

(10) International Publication Number
WO 2004/004573 A1

(51) International Patent Classification⁷: **A61B 8/06**,
5/026, A61M 1/12

Allan [AU/AU]; P O Box J241, Coffs Harbour, NSW 2450 (AU).

(21) International Application Number:
PCT/AU2003/000809

(74) Agent: **BALDWIN SHELSTON WATERS**; 60 Margaret Street, Sydney, NSW 2000 (AU).

(22) International Filing Date: 26 June 2003 (26.06.2003)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:
PS 3352 3 July 2002 (03.07.2002) AU

(71) Applicant (for all designated States except US): **USCOM PTY LTD** [AU/AU]; 323 Old Coast Road, Korora, New South Wales 2450 (AU).

(81) Designated States (*national*): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.

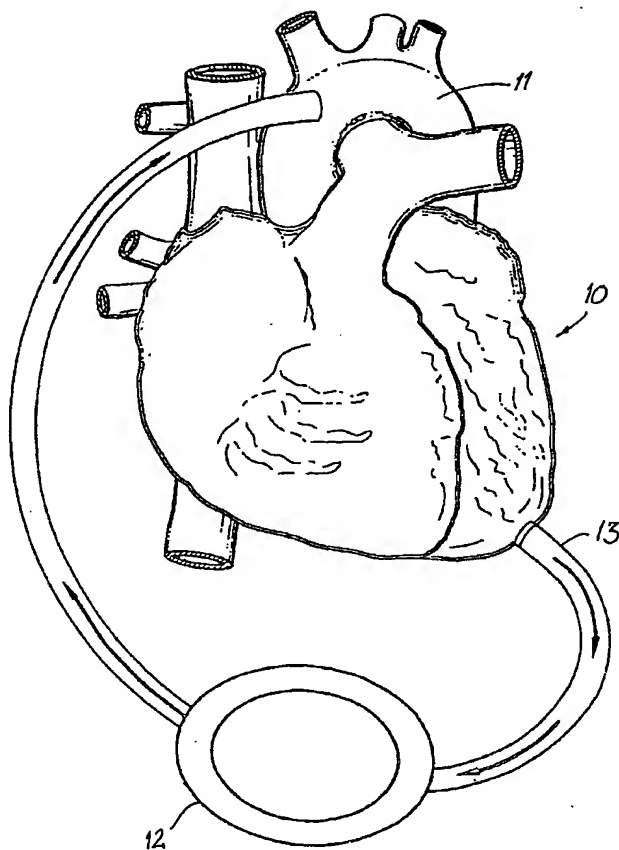
(84) Designated States (*regional*): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PT, RO,

(72) Inventor; and

(75) Inventor/Applicant (for US only): **PHILLIPS, Robert**,

[Continued on next page]

(54) Title: **PROSTHETIC HEART FUNCTION EVALUATION METHOD AND APPARATUS**



(57) Abstract: A method of monitoring or serial measurement of the operation of a prosthetic assist device (12), the method comprising the steps of: (a) utilising a non-invasive device (21) to monitor or serially measure directly the blood flow through the by-passed heart ventricle (5); (b) separately monitoring or serially measuring the blood flow through the prosthetic assist device (12); (c) combining said two measurements to determine an overall cardiac output and a native to prosthetic flow ratio.

WO 2004/004573 A1



SE, SI, SK, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Declarations under Rule 4.17:

— as to applicant's entitlement to apply for and be granted a patent (Rule 4.17(ii)) for the following designations AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, UZ, VC, VN, YU, ZA, ZM, ZW, ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG,

ZM, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PT, RO, SE, SI, SK, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG)

— of inventorship (Rule 4.17(iv)) for US only

Published:

— with international search report

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

Prosthetic Heart Function Evaluation Method and Apparatus

Field of the Invention

The present invention relates to the field of monitoring of prosthetic heart devices and in particular, it discloses a form of CW Doppler monitoring of such
5 devices.

Background of the Invention

The malfunctioning of the heart muscle is a major killer in society. Various devices have been proposed for assisting the operations of the cardiac function and stimulating the heart's natural pumping action. These heart assist devices come in
10 many forms from full heart replacement to minor forms of assist, where small pumps connected to the ventricle are mounted outside the heart, and connecting flow from the ventricle to the aorta, by-passing the ventricle and systemic aortic valve.

For a survey of the field of heart (ventricular) assist devices, reference is made to:

15 -United States Patent Application US2003/0092961 to Korakianitis publish May 15, 2003 and in particular to the references described in the Description of Related Art portion of the Application;

-United States Patent Application US2003/0088147 to Bolling et al and United States Patent Number 6428464 to Bolling and to the references referred to therein;
20 and

-United States Patent Number 6050932 to Franchi and United States Patent Number 5267940 to Muller.

In Fig. 1, there is shown a perspective view partly in section of the human heart. The heart can be divided into four chambers including the right atrium 2, the
25 right ventricle 3, the left atrium 4 and the left ventricle 5. Between the chambers 2, 3

is the tricuspid valve 6. At the exit of the right ventricle is the pulmonary valve 7. Between the two chambers 4, 5 is the mitral valve 8. At the exit to the left ventricle is the aortic valve 9.

Many different prosthetic devices exist, including complete heart replacement.

5 For example, one form of prosthetic device discussed in US Patent 6428464 amongst others bypasses the native left ventricular circulation by redirecting flow from the left ventricle 5 to the thoracic aorta 11. These prosthetic devices are designed to offload the ventricle 5 by redirecting flow from the ventricle mechanically, and encouraging the native ventricle to increase its function under
10 decreased load. Unfortunately, in practice it is difficult to determine the effectiveness of operation of such devices. It would therefore be desirable to provide for accurate flow monitoring of heart assist devices for the analysis of the proper functioning of such devices.

Summary of the Invention

15 It is an object of the present invention to provide for an improved form of monitoring of the flow through the heart in conjunction with a prosthetic assist device.

In accordance with a first aspect of the present invention, there is provided a method of monitoring or serial measurement of the operation of a prosthetic assist
20 device, the method comprising the steps of: (a) utilising a non-invasive device to monitor or serially measure directly the blood flow through the by-passed heart ventricle; (b) separately monitoring or serially measuring the blood flow through the prosthetic assist device; (c) combining said two measurements to determine an overall cardiac output and a native to prosthetic flow ratio.

Preferably, the non-invasive device monitoring comprises continuous wave Doppler flow monitoring of the heart. The monitoring can occur from a transducer placed over the parasternal acoustic access and can be repeated under a number of different operational conditions for a patient including walking and/or running.

5 Ideally, the method is repeated under a number of different physiological and pharmacological conditions for a patient.

Brief Description of the Drawings

The preferred embodiments of the present invention will now be described with reference to the accompanying drawings in which:

10 Fig. 1 is a perspective view partly in section of the human heart;

Fig. 2 illustrates schematically the operation of a prosthetic assist device;

Fig. 3 illustrates utilisation of a CW transducer device for monitoring heart function;

Fig. 4 illustrates the transducer device of Fig. 3;

15 Fig. 5 illustrates one form of output of the transducer device; and

Fig. 6 illustrates the various portions output in the arrangement of Fig. 5.

Description of the Preferred and Other Embodiments

In the preferred embodiment, accurate measurement of total ventricular function is provided by continuous wave Doppler (CW Doppler) measurement of the
20 native ventricular function in addition to accurate flow measurement through the mechanical device.

Turning initially to Fig. 2, there is illustrated a schematic of the human heart 10 which includes the aorta 11 and an additional mechanical assist device 12 which has a shunted ventricle input 13 and an aorta output 14. Whilst the flow through the

mechanical assist device 12 can often be accurately measured, the flow out of the heart 10 via aorta 11 is less accurately measurable.

In the preferred embodiment, techniques of CW measurement are utilised so as to provide for flow measurements produced by the heart.

5 Turning to Fig. 3, there is shown a patient 20 having a non-invasive sensor 21 attached to the body. The sensor 21 comprises a CW transducer device which is interconnected to a base station unit 22.

Fig. 4 shows an example of the first sensor transducer actuator 11 for attachment to the skin surface. CW Doppler measurements are utilised to monitor the blood flow through the heart. CW Doppler is a non-invasive technique in which
10 ultrasonic signals from transducer elements are directed into a blood carrying vessel of a patient. Doppler shifts in the reflected signal provide an indication of the rate of blood flow. In Fig. 2, a transducer element 21 includes an ultrasonic transducer 25 attached to a positioning device 26 which can be used to initially set the position of
15 the transducer. Between the transducer 25 and a patient's skin 27 is placed a gel coupling layer 28 for coupling the ultrasonic transducer vibrations to the skin 27. The principles of CW Doppler flow measurement are known are set out in more detail in Patent Cooperation Treaty (PCT) publication number WO 99/66835 entitled "Ultrasonic Cardiac Output Monitor" assigned to the present assignee, the contents
20 of which are incorporated herein by cross-reference. This citation describes in more detail an ultrasonic transducer device suitable for measuring blood flow within the heart using the CW Doppler method. The teaching of the above application have been embodied in an operational form in an Ultrasonic Cardiac Output Monitor available from the assignee of the present application.

In the embodiment shown in Fig. 3, the transducer elements are placed on the patient to obtain intra-cardiac or aortic signals, for example through a suprasternal notch.

The CW method detects the velocity of individual blood cells by measuring the frequency change of a reflected ultrasound beam and displaying this as a velocity time flow profile, an example of which is shown in Fig. 5. The transducer output forms an input to the processor unit 22 of Fig. 3. From the velocity time flow profile, the processor can calculate the velocity time integral (vti) and other relevant information such as heart rate (HR), each of which is illustrated in Fig. 6. The information can be derived from Fig. 6 by appropriate image processing of the CW output image.

The total systemic output, or the total volume of blood directed into the systemic vessels, is the sum of the native plus the prosthetic output. The ratio of the two flows can be denoted a native to prosthetic flow index and can be utilised to determine appropriate levels for setting the prosthetic output of the prosthetic device 12 of Fig. 2.

Preferably, after fitting the heart assist device, the performance of the device relative to heart rate measurements are conducted under a number of different conditions.

Through measuring the device performance for a wide range of patients under a wide range of different conditions, an extensive database can be constructed of optimal performance conditions for utilisation of the heart assist device. In this way, the heart assist device can be tuned for sophisticated operation.

Further, the utilisation of the index and extensive measurements allows for optimisation of pharmacotherapy. The monitoring device thereby provides the

ability to accurately monitor output flow from the heart function with potential therapeutic benefits.

Further, where the heart assist device does not include its own flow measurement capabilities, its input or output can be separately examined by the
5 ultrasound transducer device so as to determine the assist device's output level.

It will be understood that the invention disclosed and defined herein extends to all alternative combinations of two or more of the individual features mentioned or evident from the text or drawings. All of these different combinations constitute various alternative aspects of the invention.

10 The foregoing describes the embodiments of the present invention and modifications, obvious to those skilled in the art can be made thereto, without departing from the scope of the present invention.

THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:-

1. A method of monitoring the operation of a prothetic assist device, the method comprising the steps of:

(a) utilising a non invasive device to monitor or serially measure directly the

5 blood flow through at least one heart ventricle;

(b) separately monitoring the blood flow through the prothetic assist device;

(c) combining said two measurements to determine an overall native to
prosthetic flow index.

2. A method as claimed in claim 1 wherein said non invasive device monitoring or
10 serial measurement comprises continuous wave Doppler flow monitoring of the
heart.

3. A method as claimed in claim 1 wherein the heart is monitored or serially
measured from a transducer placed adjacent the suprasternal notch.

4. A method as claimed in claim 1 wherein said method is repeated under a
15 number of different operational conditions for a patient including walking and/or
running.

5. A method as claimed in claim 1 wherein said method is repeated under a
number of different pharmalogical conditions for a patient.

1 / 6

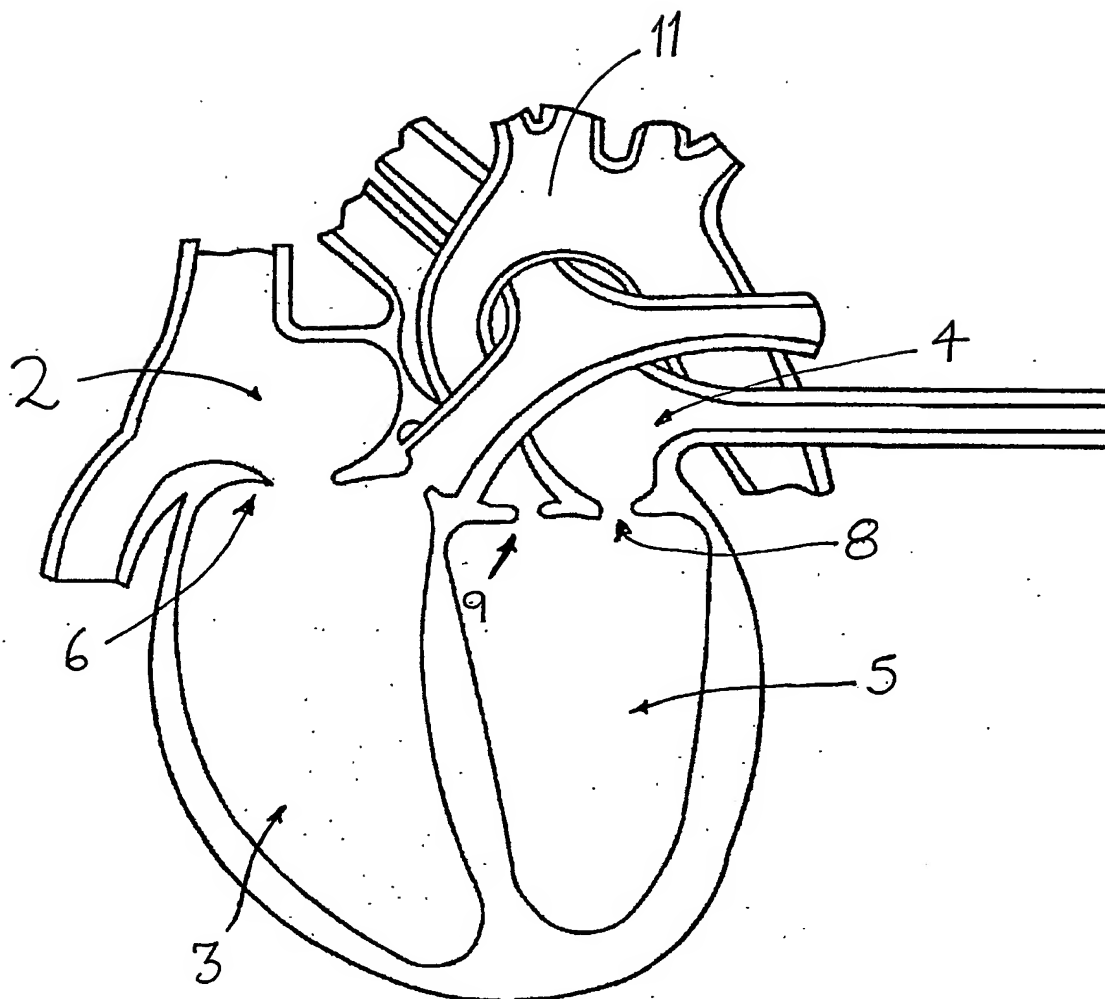


FIG. 1

2 / 6

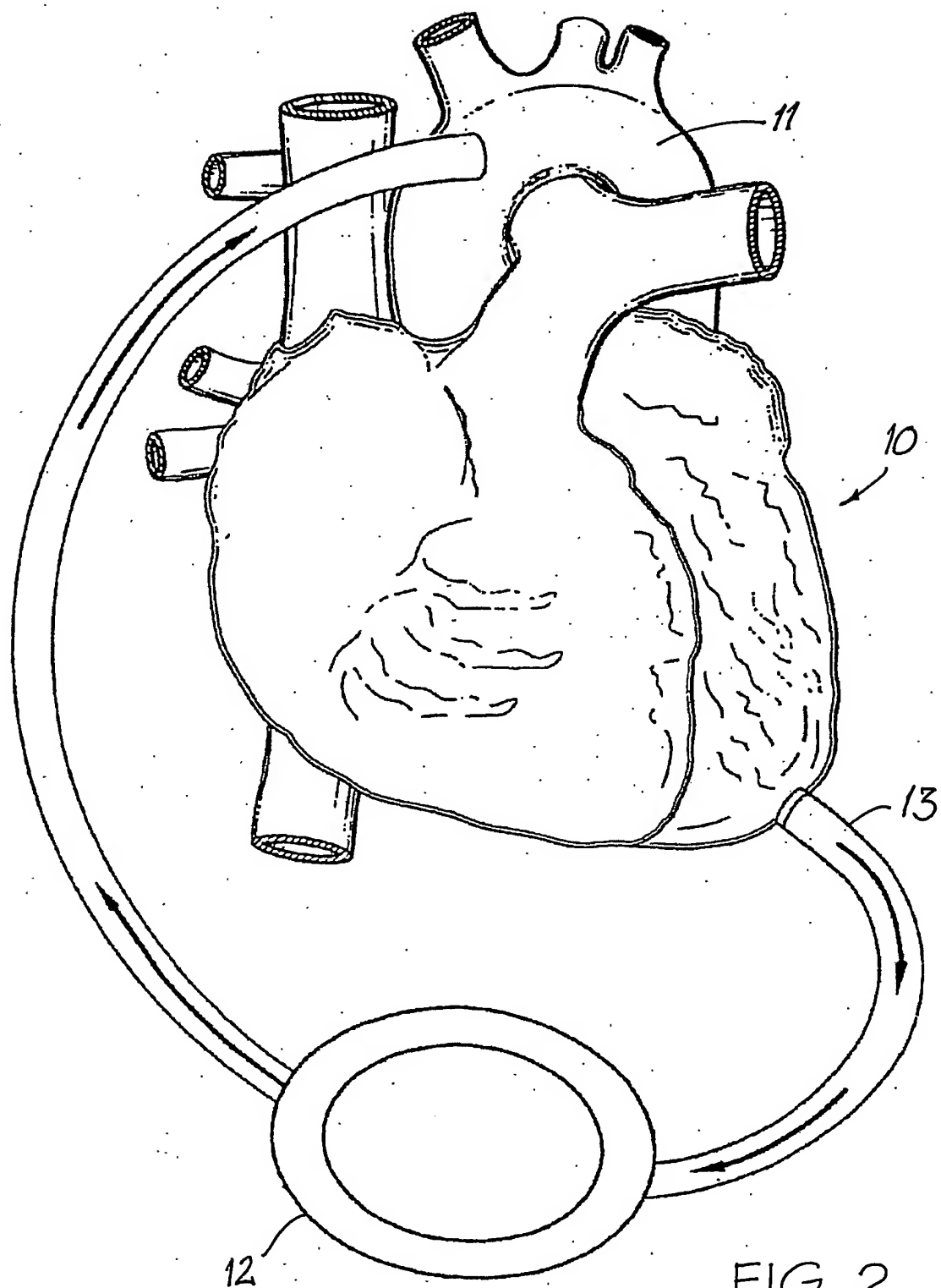
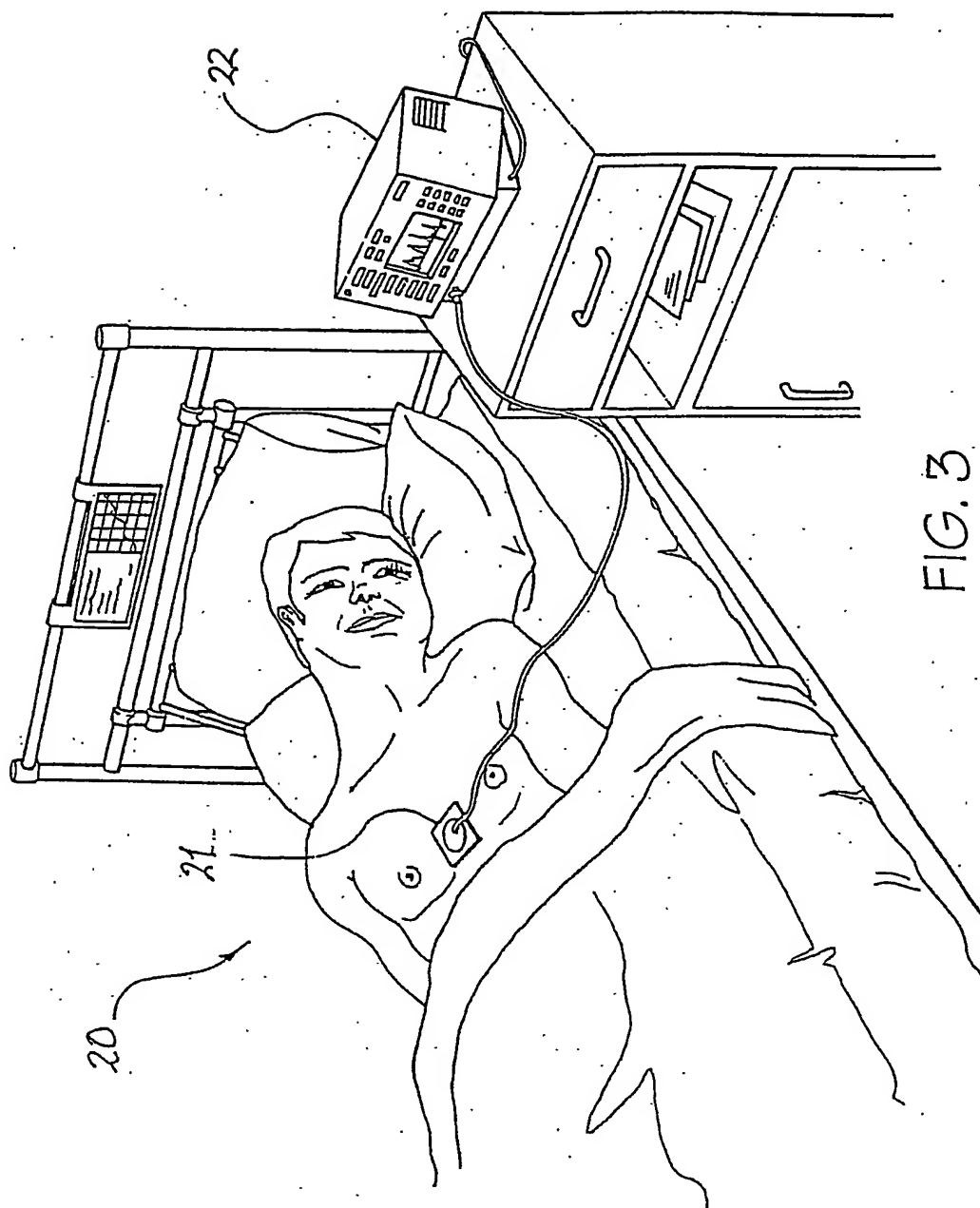


FIG. 2

3 / 6



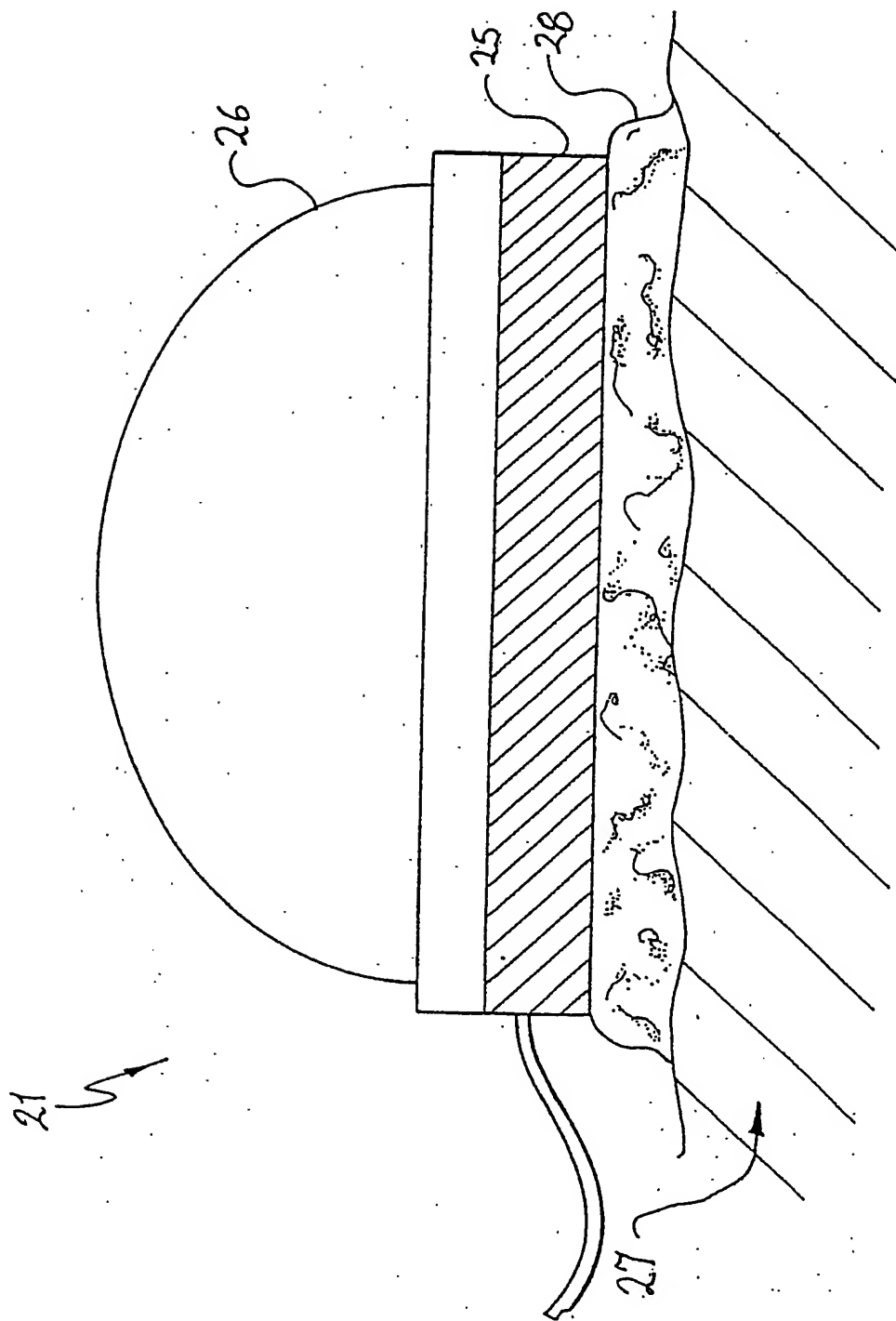
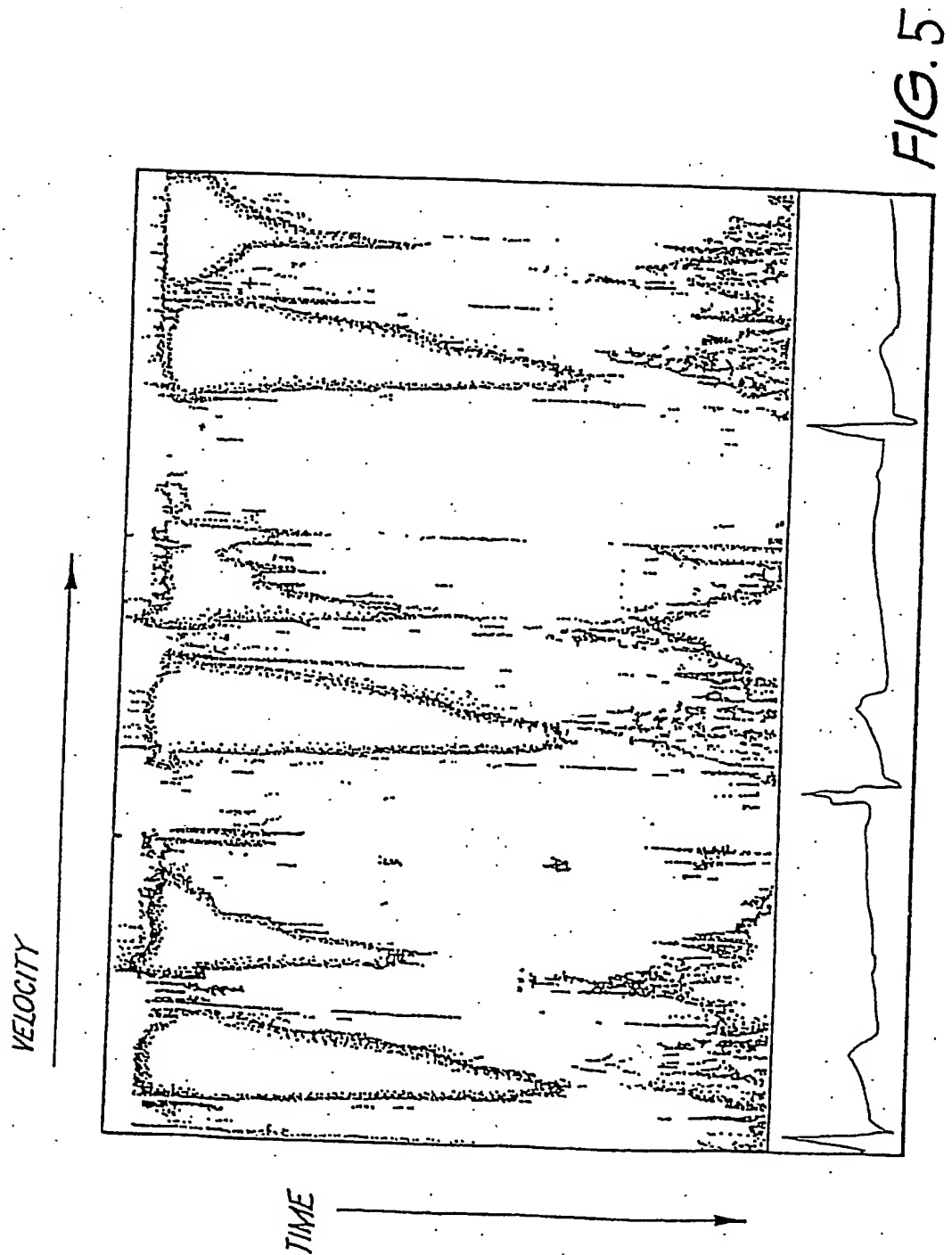


FIG. 4

5 / 6



6 / 6

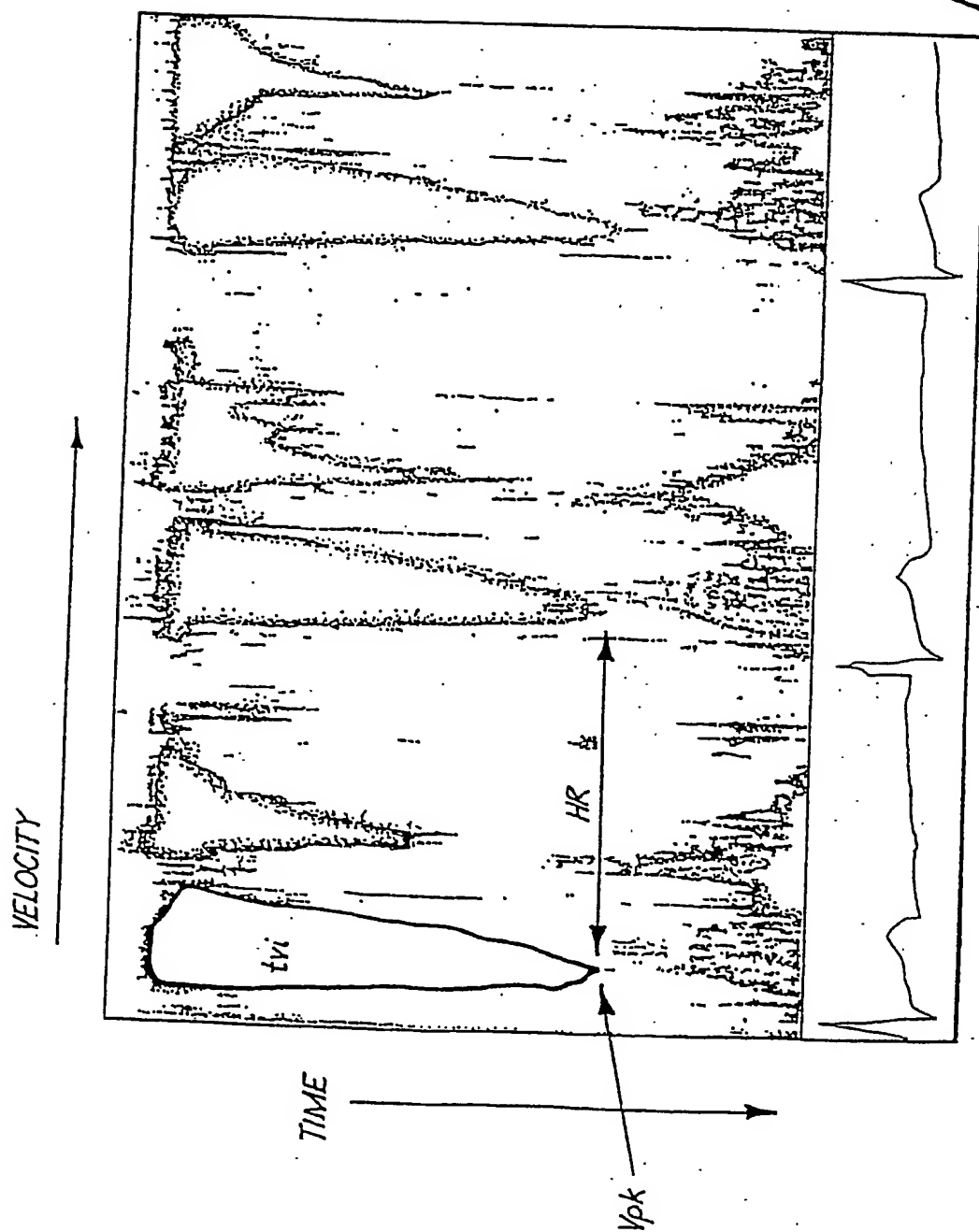



FIG. 6

INTERNATIONAL SEARCH REPORT

International application No.
PCT/AU03/00809

A. CLASSIFICATION OF SUBJECT MATTER		
Int. Cl. ⁷ : A61B 8/06, 5/026, A61M 1/12		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols)		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used) DWPI + keywords(a61m1/12,a61b5/-,a61b8/-,cardio,heart,prosthe,artificial,ventric,flow,performance etc.)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5313947 A1 (MICCO) 24 May 1994	All
A	WO 01/48451 A1 (APEX MEDICAL INC.) 5 July 2001	All
A	US 5139020 A1 (KOESTNER et al.) 18 August 1992	All
P,A	WO 03/015609 A2 (APEX MEDICAL, INC.) 27 February 2003	All
<input type="checkbox"/> Further documents are listed in the continuation of Box C <input checked="" type="checkbox"/> See patent family annex		
<p>* Special categories of cited documents:</p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier application or patent but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art</p> <p>"&" document member of the same patent family</p>		
Date of the actual completion of the international search 30 September 2003		Date of mailing of the international search report 9 OCT 2003
Name and mailing address of the ISA/AU AUSTRALIAN PATENT OFFICE PO BOX 200, WODEN ACT 2606, AUSTRALIA E-mail address: pct@ipaustalia.gov.au Facsimile No. (02) 6285 3929		Authorized officer  JONATHAN MILLS Telephone No : (02) 6283 2113

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No.

PCT/AU03/00809

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report		Patent Family Member	
US	5313947	US	4819652
WO	0148451	AU	18087/01
US	5139020		
WO	03015609	US	2003045772
END OF ANNEX			